Ball & Cage Prosthetic Valve! An Obsolete Giant!
Muhammad Rafique, M.D.\textsuperscript{a,c}, Sarah Hamid, M.D.\textsuperscript{b}, Landai Nguyen, D.O.\textsuperscript{a},
Grace Wenzel, M.D.\textsuperscript{c}, Bassam Omar, M.D., Ph.D.\textsuperscript{a}

Description

The cine still images and video show a ball and cage (Starr Edwards) aortic prosthetic valve in the open position in systole (A) and in the closed position in diastole (B). This type of prosthesis, once a giant in valve replacement surgery, is currently obsolete due to the high turbulent non-laminar flow, largely overcome by the more recent tilting disk valve prosthesis design.

The need for prosthetic heart valves was recognized long time ago, but the idea remained wishful and initially impractical. In 1912, Dr. Theodore Tuffier used his finger to free the fused leaflets of a stenosed aortic valve [1]. This was the first “closed heart procedure.” He was able to dilate the valve by pushing the invaginated aortic wall through the stenotic aortic valve.

In 1952 Dr. Charles Hufnagel implanted an acrylic ball encased in Lucite into the descending aorta of a 30 years old woman to correct aortic insufficiency at Georgetown Medical center, Washington D.C [2,3]. This was an initial step of a long journey more than half a century ago. Greater than 200 implanted Hufangel valves functioned for as long as 30 years with no significant wear; without use of anticoagulation. The downside of this design was that it could only be placed in the descending aorta instead of heart itself. It carried high mortality rate and the implantation procedure was cumbersome. Patients could hear the plastic ball bouncing inside their chest. Later, a hollow nylon ball coated with silicone rubber was used which reduced the valve noise. Although it had poor hemodynamic profile and could only give symptomatic relief, it proved that synthetic materials could be used to develop heart valves [4].

It was the development of the heart-lung machine in 1953 by Dr. John Gibbon at Thomas Jefferson hospital in Philadelphia that allowed cardiac surgery to blossom. In 1960, Dr. Harkins and his colleagues from Rhode Island started the modern era of prosthetic aortic valve replacement by inserting a double caged-ball valve into the aortic orifice below coronary ostia following the excision of diseased cusps [5].

Manuscript submitted July 28, 2019, accepted August 8, 2019.

\textsuperscript{a} Division of Cardiology, University of South Alabama, Mobile, AL, USA

\textsuperscript{b} Penn Highlands Healthcare, DuBois, PA, USA

\textsuperscript{c} Corresponding Author: Muhammad Rafique, MD, Division of Cardiology, University of South Alabama, 2451 USA Medical Center Dr., Mobile, AL 36617, USA.

Email: mrafique@health.southalabama.edu

the mid1960s, Albert Starr (a physician) and Lowell Edwards (an electrical engineer) simplified the caged-ball valve by using a single titanium cage, a silastic ball and a sewing ring covered with Teflon. This Starr-Edwards valve was first implanted in the mitral position in 1960 and later in the aortic position. It had a sewing ring which was easy to suture to the aortic annulus [6]. The caged-ball valves, however, had a non-physiologic hemodynamic profile. The central ball occluder caused lateralization of forward flow with high turbulence; and the large sewing ring resulted in a restricted effective orifice area [7].

In 1969 tilting-disk mechanical prostheses were developed which had more physiologic central flow. The Björk-Shiley valve was the first tilting-disk prosthesis that was widely used. It was designed with a central disk held in place by two struts. The open valve had two orifices and resistance to blood flow was related to disk design and degree of opening angle. The disk design was progressively modified into a convexo-concave shape that could slide about 2 mm during its movement, increasing the effective orifice area [8]. Björk-Shiley valves were recalled due to fracture of welded struts.

In 1977 bileaflet prostheses were developed by St. Jude Medical which consisted of two semicircular disks. This design produced three flow areas with a more uniform and laminar central flow. These valves provide greater effective orifice area and are least thrombogenic in comparison to other prosthetic valves [9,10]. In 1996, the On-X valve bileaflet tilting disk prosthesis was introduced with a more laminar flow design and less thrombogenicity, requiring lower anticoagulation targets [11].

References:


KEYWORDS: Prosthetic Valves; Valvular Disease; Valve Replacement

Reference this article as: